Measuring the Transmission Matrix in Optics: An Approach to the Study and Control of Light Propagation in Disordered Media

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We introduce a method to experimentally measure the monochromatic transmission matrix of a complex medium in optics. This method is based on a spatial phase modulator together with a full-field interferometric measurement on a camera. We determine the transmission matrix of a thick random scattering sample. We show that this matrix exhibits statistical properties in good agreement with random matrix theory and allows light focusing and imaging through the random medium. This method might give important insight into the mesoscopic properties of a complex medium.

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The propagation of waves in heterogeneous media, especially in the multiple-scattering regime, is a very fundamental problem of physics with numerous applications ranging from solid-state physics and optics, to acoustics and electromagnetism [1]. The behavior of such media is usually described by their average macroscopic properties which can be obtained through intensity measurements using, for example, speckle pattern correlations [2] or coherent back scattering experiments [3,4].

A deeper approach for the study of complex media lies in the transmission matrix (TM) retrieval. This matrix is a subpart of the usual scattering matrix as defined in [5] for instance. Within this framework, the Green’s function between an array of sources and an array of sensors is recorded in transmission. The knowledge of the TM brings more fundamental insight into the medium. One can for instance extract from the TM the single and the multiple-scattering component [6], the backscattering cone, and the field-field correlations [7,8]. The distribution of the singular values of the TM should also be related to the diffusion properties and might exhibit a coherence effect beyond the diffusive transport regime such as weak and strong localization effects.

Furthermore, from an operative point of view, the knowledge of the TM of a complex medium offers new and exciting possibilities. For instance, using Time Reversal (TR), it has been shown that multiple scattering, far from limiting wave manipulation through a random medium, can in fact greatly enhance it. Such approaches, which are based on the reciprocity and the reversibility of the wave equations [9], have proved very useful in various areas ranging from focusing to imaging or telecommunication, in acoustic [10–12], electromagnetic [13,14] or even seismology [15].

For acoustic (electromagnetic) waves, transducers (antennas) are natural local receivers and emitters in phase and amplitude, and oscillation frequencies are compatible with electronic detection. Therefore, the TM can be straightforwardly measured. In contrast, reconstructing the transmission matrix of a complex medium is still an elusive problem in the optical domain.

Nonetheless some recent experiments have demonstrated that it is possible to manipulate light at a mesoscopic level in a complex medium in order to focus light through [16] or in [17] a scattering medium, as well as couple efficiently to the open channels of a disordered sample [18]. These experiments were made possible by the emergence of spatial light modulators (SLM).

In the present Letter, using a SLM alongside a full-field interferometric method, we demonstrate that we are able to measure the monochromatic transmission matrix of a random multiple-scattering medium. We first detail the experimental setup of the TM evaluation method. In a second part, we show that the knowledge of the TM allows one to reproduce the results of [16], make the link with TR experiments [11,14], and allows detection of an unknown object after propagation through the scattering media. Finally, we study the statistical properties of the singular values of the TM, and show that it follows a quarter-circle law typical of a random wave field.

We define the mesoscopic TM of an optical system for a given wavelength as the matrix \( K \) of the complex coefficients \( k_{mn} \) connecting the optical field (in amplitude and phase) in the \( m \)th output free mode to the one in the \( n \)th input free mode. Thus, the projection \( E_{m}^{\text{out}} \) of the outgoing optic field on the \( n \)th free mode is given by \( E_{m}^{\text{out}} = \sum_{n} k_{mn} E_{n}^{\text{in}} \), where \( E_{n}^{\text{in}} \) is the complex amplitude of the optical field in the \( n \)th incoming free mode.

The sample under study is an opaque 80 ± 25 \( \mu \)m thick deposit of ZnO (Sigma-Aldrich 96479) on a microscope slide. The experimental setup consists of a single longitudinal mode laser source at 532 nm (Laser Quantum Torus), a modulation part to illuminate the sample with a controlled wave front and a detection part to measure the optical intensity transmitted by the scattering medium. The laser beam is first expanded then spatially modulated by the SLM. This modulator is a twisted nematic liquid crystal on silicon device (Holoeye LC-R 2500). Choosing a suitable combination of incident and analyzed polariza-
tions, we achieve an almost phase-only modulation \cite{19} with a $2\pi$ modulation in phase and a maximum residual intensity modulation below 10%. The surface of the SLM is imaged on the pupil of a 20x objective with a numerical aperture (NA) of 0.5, thus a pixel of the SLM matches a wave vector at the entrance of the scattering medium. The beam is focused at one side of the sample and the output intensity speckle is imaged 0.3 mm from the surface of the sample by a 40x objective (NA = 0.85) onto a CCD camera (AVT Dolphin F-145B). The speckle is stationary well over the measurement time (several minutes).

We choose the size of the input and output independent pixels to have a perfect matching in size between a pixel and a mode, in particular, a CCD pixel has the size of a speckle grain. Thus, in our setup, the input and output modes are the SLM and the CCD pixels, respectively, and the TM corresponds to the system comprised of both the scattering sample and the optical system between the SLM and the CCD camera. From now on, we fixed both the scattering sample and the optical system between the SLM and the CCD and the TM corresponds to the system comprised of both the scattering sample and the optical system between the SLM and the CCD camera. From now on, we fixed both the number of controlled segments on the SLM and the number of subdivisions measured on the observation window of the CCD to $N = 256$.

To access the complex optical field, we used interferences with a known wave front and a full field “four phases method” \cite{20}. For any input vector, if the relative phase is shifted by a value $\alpha$, the intensity in the $m$th output mode is given by

$$I_m^{\alpha} = |E_m^{\alpha}|^2 = \left| s_m + \sum_n e^{i\alpha k_{mn} E_n^{\alpha}} \right|^2 = |s_m|^2 + \left| \sum_n e^{i\alpha k_{mn} E_n^{\alpha}} \right|^2 + 2|s_m|\left| \sum_n k_{mn} E_n^{\alpha} \right|,$$

where $s_m$ is the complex amplitude of the optical field used as reference in the $m$th output mode.

Thus, if we inject the $n$th input mode and we measure $I_m^{0}, I_m^{\pi/2}, I_m^{\pi}, I_m^{3\pi/2}$, respectively, the intensities in the $n$th outgoing mode for $\alpha = 0, \pi/2, \pi, 3\pi/2$, and we compute $(I_m^{0} - I_m^{\pi})/4 + i(I_m^{\pi/2} - I_m^{3\pi/2})/4 = \bar{s}_m k_{mn}$.

For practical reasons, we choose the Hadamard basis as input basis over the canonical one, whose elements are either +1 or −1 in amplitude. It perfectly fits with the use of a phase-only SLM and it also maximizes the measured intensity and consequently improves the experimental signal to noise ratio (SNR) \cite{21}. For all Hadamard basis vectors, the intensity is measured on the canonical basis of the pixels on the CCD camera and an observed transmission matrix $K_{obs}$ is acquired, which is related to the real one $K$ by $K_{obs} = K \times S_{ref}$, where $S_{ref}$ is a diagonal matrix representing the static reference. Ideally, the reference wave front should be a plane wave to directly have access to $K$. In this case, all $s_m$ are constant and $K_{obs}$ is directly proportional to $K$. However this requires the addition of a reference arm to the setup, as well as interferometric stability. To have the simplest experimental setup and a higher stability, we modulate only 65% of the wave front going into the scattering sample (this corresponds to the square inside the pupil of the microscope objective as seen in Fig. 1), the speckle coming from the 35% static part being our reference. $S_{ref}$ is now unknown and no longer constant along its diagonal. Nevertheless, since $S_{ref}$ stationary over time, we can measure the response of all input vectors on the $m$th output pixel as long as the reference speckle is bright enough on the considered modes. We will quantify the effect of the reference speckle and show that neither does it impair our ability to focus or image using the TM, nor does it affects the statistical properties of the TM.

A good way to confirm the physical relevance of the TM is to use it to focus light on any desired outgoing mode. In \cite{11,14}, it was demonstrated that using time reversal, one can take advantage of multiple scattering to focus on tight spots. TR being a matched filter \cite{11}, the energy is maximized both temporally and spatially at the intended location. The monochromatic equivalent of TR is phase conjugation, which can be straightforwardly done using our acquired TM. We expect similar focusing results as in \cite{16}, which were obtained through a procedure that ensures an optimum phase-modulated wave front maximizing the energy of a given mode. Denoting $E_{target}$ the output target vector, the input vector that approximates the desired pattern at the output for a perfect phase conjugated focusing is given by $E_{in} = K^\dagger E_{target}$, where $\dagger$ stands for the conjugate transpose. Thus, the theoretical effective output vector is $E_{eff} = O_{foc}^\dagger E_{target}$ where $O_{foc} = KK^\dagger$ is the so-called time reversal operator \cite{22}. Since our setup is limited to phase modulation only, and given the fact that we do not acquire $K$ but $K_{obs}$, the input vector for a given output target reads

$$E_{in}^{\alpha} = K_{obs}^{\dagger} E_{target}^{\alpha} / |K_{obs}^{\dagger} E_{target}^{\alpha}|.$$  

We use the setup shown in Fig. 1 to record the transmission matrix of our system, which is done in approximately 3 min (and requires 4N measurements), comparable to the time needed to perform an iterative focusing as

\begin{figure}[h]
\centering
\includegraphics[width=\columnwidth]{fig1.png}
\caption{(color online). Schematic of the apparatus. The laser is expanded and reflected off a SLM. The phase-modulated beam is focused on the multiple-scattering sample and the output intensity speckle pattern is imaged by a CCD camera: lens (L), polarizer (P), diaphragm (D).}
\end{figure}
described in [16]. A speckle spot is chosen as the intended target, and we use formula (2) to perform phase conjugation. The results obtained are shown in Fig. 2. We estimated the experimental SNR defined by the ratio of the intensity at the focus to the mean intensity of the speckle outside. In Fig. 2(b), the result of the focusing on this single spot shows a SNR$_{\text{exp}} = 54$ which in par the results of the focusing technique used in [16].

It is important to quantify the effect of both the phase-only modulation and the reference speckle used to acquire the TM of our complex medium. Indeed, rather then $O^\text{foc}$, the effective focusing operator includes a normalization to take into account the phase-only modulation. For a single spot focusing, $O^\text{foc \_norm} = K_\text{obs} K^\dagger_\text{norm}$ where $k^\text{norm} = k_{ij}/|k_{ij}|$.

In the representation of the focusing operator $O^\text{foc \_norm}$ [Fig. 2(c)], each line corresponds to the expected output intensity image while focusing on any point of the CCD’s observation window. The strong diagonal proves our ability to focus light on any of these spots. As an example Fig. 2(d) shows focusing on 3 spots. It is worth noting that $O^\text{foc \_norm}$ presents weaker subdiagonals which are due to correlations between neighboring pixels. Finally, we would like to emphasize that the strong advantage of this focusing technique, compared to a sequential algorithm, is that it is not necessary to acquire anymore information to focus on different or multiple spots in one step.

From a theoretical point of view, monochromatic phase conjugation focusing through a multiple-scattering medium has been studied in Derode et al. [23]. The general formulation for the efficiency of this focusing is $\text{SNR} = N_{\text{grains}}$ the total number of “information grains”, or degrees of freedom. In our case, this number is the number of independent pixels (or channels) which is the number $N$ of pixels controlled. In our experiment, the use of a reference speckle limits the number of degrees of freedom. Denoting $\gamma$ the fraction of the SLM used to acquire the TM, and using the theoretical formalism developed in [23] the effective SNR including the effect of the reference writes $\text{SNR}_\text{ref} = \pi/4(\gamma N + (1 - \gamma)/\gamma) = 0.8\gamma N \forall N \gg 1$. Here $(1 - \gamma)/\gamma$ is the effect of the reference speckle which contributes as noise at the focal spot, and the prefactor is due to the phase-only modulation [16,24]. The experimental SNR of the focusing shown in Fig. 2(b) is 41% of SNR$_\text{ref}$, with $\gamma = 65\%$.

We have shown that the TM of the medium is a powerful tool that can be used to focus through a medium, but we want to emphasize here that it extends well beyond focusing. An example is the detection of an amplitude or phase object placed at the entrance of the scattering sample. Because of the spatial reciprocity of wave propagation inside the scattering medium, the detection issue is reciprocal to the focusing one. Once the matrix is measured, one can retrieve the initial input $E^\text{obj}$ from the output speckle $E^\text{out}$. Indeed, the reconstructed image reads $E^\text{img} = K_\text{obs}^\dagger E^\text{out} = O^\text{foc \_norm} E^\text{obj} = O^\text{foc} E^\text{obj}$ which is almost equivalent to the result obtained in a focusing scheme since $O^\text{foc}$ has the same statistical properties than $O^\text{foc \_norm}$ but without the phase-only effects. In order to demonstrate the validity of this approach we performed the following detection experiment: instead of placing an object between the SLM and the medium, the object is generated by the SLM itself using two phase masks $E^{(1)}_\text{obj}$ and $E^{(2)}_\text{obj}$. The mask $E^{(1)}_\text{obj}$ is a plane phase and $E^{(2)}_\text{obj}$ is obtained by flipping the phase of $N_{\text{obj}}$ pixels from 0 to $\pi$. The amplitude $E^{(1)}_\text{out}$ and $E^{(2)}_\text{out}$ of the output speckles are measured. The virtual object $E^{(1)}_\text{obj} - E^{(2)}_\text{obj}$ is an amplitude object, recovered by calculating $E^\text{img} = K_\text{obs}(E^{(1)}_\text{out} - E^{(2)}_\text{out})$. It gives the images that would be obtained if an opaque screen drilled with $N_{\text{obj}}$ holes was placed at the pupil of the input microscope objective. The results of this operation are shown in Fig. 3 for $N_{\text{obj}} = 1$ and $N_{\text{obj}} = 2$. It is clear that a simple object placed at the input of the sample can be reconstructed after propagation, regardless of the randomness of the medium. Considering that this imaging method is reciprocal of the focusing one, the detection is achieved with the same SNR.

These experimental focusing and detection experiments through a multiple-scattering sample are clear demonstrations that the measured transmission matrix is physical, i.e., effectively links the input optical field to the output one. Theoretically, this matrix is related to the scattering matrix and should be an extremely powerful tool for the study of random and complex media. As a first step in this direction, we performed the simplest analysis of the TM: a singular value decomposition. Indeed, provided that there is no ballistic wave in the field at the output of the sample.
random matrix theory (RMT) predicts that for those matrices the statistical distribution $\rho(\tilde{\lambda})$ follows the so-called “quarter-circle law” where $\tilde{\lambda}$ are the singular values (SV) normalized by the total intensity $[25]$. The effect of the diagonal matrix $S_{\text{ref}}$ on $K$ is to multiply each line by a value $s_{jj}$. This changes the variance of the SV distribution. To remove this effect, we estimate the absolute values of $S_{\text{ref}}$ by averaging $K_{\text{obs}}$ along every line. We obtain the diagonal matrix $S_{\text{abs}}$ defined by $s_{jj}^{\text{abs}} = \langle |k_{ij}^{\text{abs}}| \rangle$ for $\langle |k_{ij}| \rangle = 1$. $S_{\text{abs}}$ has no zero on the diagonal thanks to the finite pixel size. We filter the $K_{\text{obs}}$ matrix and obtain $K_{\text{fil}} = K \times S_{\text{ref}} / S_{\text{abs}} \approx K \times \Sigma_\phi$.

Now, $\Sigma_\phi$ is a unitary matrix since it is a diagonal matrix of complex numbers of norm 1, corresponding to the unknown phase of the reference speckle. Thus the singular values of $K_{\text{fil}}$ are the same as those of $K$. We finally remove one element out of two to suppress interelement correlations between nearby pixels. Results of SV distribution of the observed matrix after filtering and down-sampling are shown in Fig. 4, the final matrix obtained follows correctly the expected quarter-circle law. This distribution differs from the bimodal one predicted by $[26]$ since there is no total energy conservation condition as the transmission matrix measured is a small part of the whole scattering matrix.

To conclude, we have demonstrated how the optical transmission matrix of multiple-scattering media can be measured using a spatial light modulator and a full-field interferometric measurement. We proved the validity of the measured TM through focusing and detection experiments. Finally, the singular value distribution was shown to follow a quarter-circle law, characteristic of random matrices. We believe that this technique will have many applications ranging from detection and imaging in random and scattering media to very fundamental problems associated with the propagation of waves in disordered systems.

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